

PHAR 7633 Basic Pharmacokinetics

Chapter 20

Non Compartmental Analysis

Typical Clinical Publication:

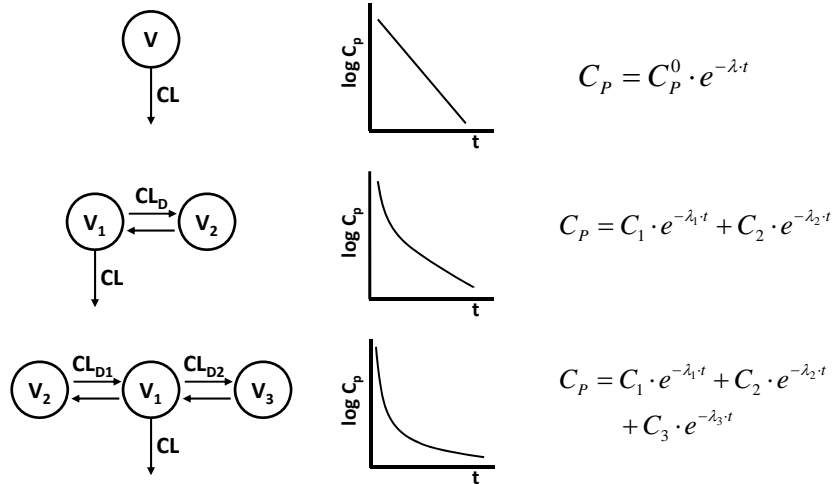
Wong SL et al., *Clin. Pharmacol. Ther.* 73: 304 (2003)

Pharmacokinetics and pharmacodynamics of abarelix, a gonadotropin-releasing hormone antagonist, after subcutaneous continuous infusion in patients with prostate cancer.

“Noncompartmental pharmacokinetics analysis. Pharmacokinetic parameters of abarelix, including maximum plasma drug concentration (C_{max}), time to reach C_{max} (T_{max}), area under the plasma concentration-time curve (**AUC**), apparent total volume of distribution during the terminal elimination phase (V_d/F) were estimated for each patient by standard noncompartmental methods. The average plasma concentration (C_{avg}) was calculated as $AUC(0-t)/\text{Duration of infusion}$, in which $AUC(0-t)$ was defined as AUC from time 0 to the last measurable concentration. The area under the first moment curve (**AUMC**) was calculated with use of the trapezoidal rule. The subcutaneous mean residence time (MRT_{sc}) of abarelix after continuous subcutaneous infusion was calculated as $AUMC/AUC - \text{Infusion time}/2$.

All of the pharmacokinetic calculations were performed with WinNonlin (version 3.3; Pharsight Corp., Mountain View, CA)”

THE PROBLEM: Many Models and Curves



Number of compartments = Number of curve exponentials.

THE QUEST: Capture Parameters Relevant to All Models and Drugs

Essential:

F : Bioavailability

CL: Clearance

V_{ss} : Steady-State Volume

Others:

V_c : Central Volume

$t_{1/2\beta}$: Terminal Half-life

THE ANSWER: Moment Analysis

Definition for a continuous function, $f(t)$; (t = time)

$$M_n = \int_0^{\infty} t^n \cdot f(t) \cdot dt$$

<u>Moment</u>	<u>Statistics</u>	<u>Physics</u>	<u>Pharmacokinetics</u>
M_0	Numbers	Weight	AUC
M_1	Mean	Center of Mass	Mean Residence Time, AUMC
\vdots			

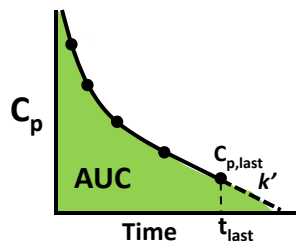
☐ Non Compartmental Analysis:

Calculate the areas of the C_p versus time curve (AUC; zero moment) and the first moment ($t \cdot C_p$) curve (AUMC) using the trapezoidal rule without making any assumption concerning the number of compartments.

Moment Functions in PK: **AUC**

$$M_0 = \int_0^{\infty} t^0 \cdot C_p dt = \int_0^{\infty} C_p dt = AUC$$

☐ Numerical Calculation:



$$AUC = \underbrace{AUC_{0-t_{last}}}_{\text{Calculated Interval Areas (Trapezoidal Rule)}} + \underbrace{\frac{C_{p,last}}{k'}}_{\text{AUC}_{(last-\infty)} \text{ (Extrapolate from } t_{last} \text{ to } t=\infty)}$$

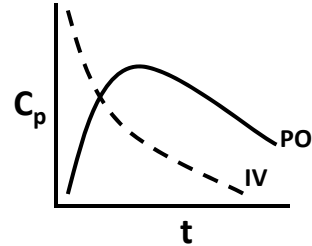
where k' is the terminal slope from semi-log graph of C_p vs. time

Utility of AUC

☐ Bioavailability (F)

The fraction of the dose available to the systemic circulation

$$F = \frac{AUC_{PO} \times Dose_{IV}}{AUC_{IV} \times Dose_{PO}}$$



☐ Total Clearance (CL)

$$CL = Dose/AUC$$

$$CL = \frac{dA_e / dt}{C_p} = \frac{\text{Elimination Rate}}{C_p}$$

$$\text{Thus : } \frac{dA_e}{dt} = CL \cdot C_p \quad \text{Rearrange}$$

$$\text{Integrate : } \int_0^\infty dA_e = CL \cdot \int_0^\infty C_p \cdot dt$$

$$A_e^\infty = Dose = CL \cdot AUC$$

Does not depend on shape of IV disposition curve.
Requires elimination from plasma compartment.

Moment Functions in PK: **AUMC**

$$M_1 = \int_0^\infty t \cdot C_p dt = AUMC$$

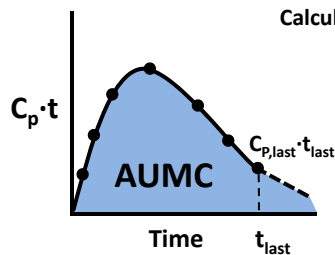
☐ Numerical Calculation:

$$AUMC = AUMC_{0-t_{last}} + \frac{C_{P,last} \cdot t_{last}}{k'} + \frac{C_{P,last}}{k'^2}$$

Calculated Interval Areas
(Trapezoidal)

$AUMC_{(last-\infty)}$
(Extrapolation)

where k' is the terminal slope from
semi-log graph of C_p vs. time



AUMC: Area under the first moment curve

$$\text{Numerical Calculation of AUMC: } = \int_0^{\infty} t \cdot C_p dt$$

Table from: <http://www.boomer.org/c/p4/c20/c2001.html>

Time (hr)	Cp (mg/L)	Cp • t (mg.hr/L)	AUC (mg.hr/L)	AUMC (mg.hr ² /L)
0	8	0	0	0
1	7.09	7.09	7.55	3.55
2	6.29	12.58	14.24	13.39
3	5.58	16.74	20.18	28.05
4	4.95	19.80	25.45	46.32
6	3.89	23.34	34.29	89.46
9	2.71	24.39	44.19	161.06
12	1.89	22.68	51.09	231.67
18	0.92	16.56	59.52	349.39
24	0.44	10.56	63.60	430.75
∞			67.27	549.31

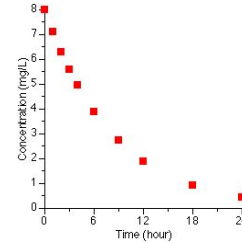


Figure 20.1.1 Plot of Cp vs Time (IV)

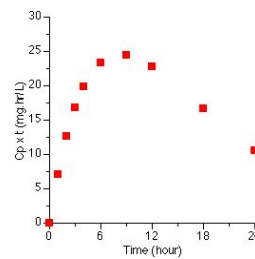


Figure 20.1.2 Plot of Cp x t vs Time (IV)

Utility of AUMC

$$MRT = \frac{AUMC}{AUC}$$

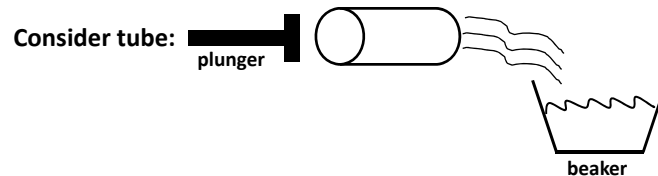
- MRT: Mean Residence Time, the average time that drug molecules remain in the body after dosing.
- Apparent elimination rate constant (kel')

$$kel' = \frac{1}{MRT} \quad \text{for an IV dose of drug}$$

- Used for calculation of other parameters, particularly $V_{ss} = MRT \cdot CL$

Noncompartmental Generation of V_{ss}

Volume of Distribution: $V_{ss} = CL \cdot MRT$



If 1 mL leaves in 1 sec: $CL = 1 \text{ mL/sec}$

If it takes 10 sec for plunger to traverse tube: $MRT = 10 \text{ sec}$

Then tube V must be: $10 \text{ sec} \times 1 \text{ mL/sec} = 10 \text{ mL}$

Hamilton Flow/Volume Principle (1931).

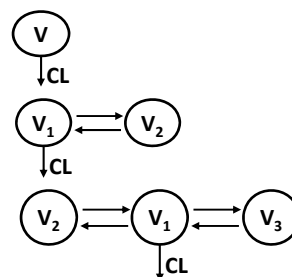
V_{ss} : All Methods Yield Equivalent Values

- V_{ss} : Compartment Models

1 CMT $V_{ss} = V$

2 CMT $V_{ss} = V_1 + V_2$

3 CMT $V_{ss} = V_1 + V_2 + V_3$



- Noncompartment Analysis

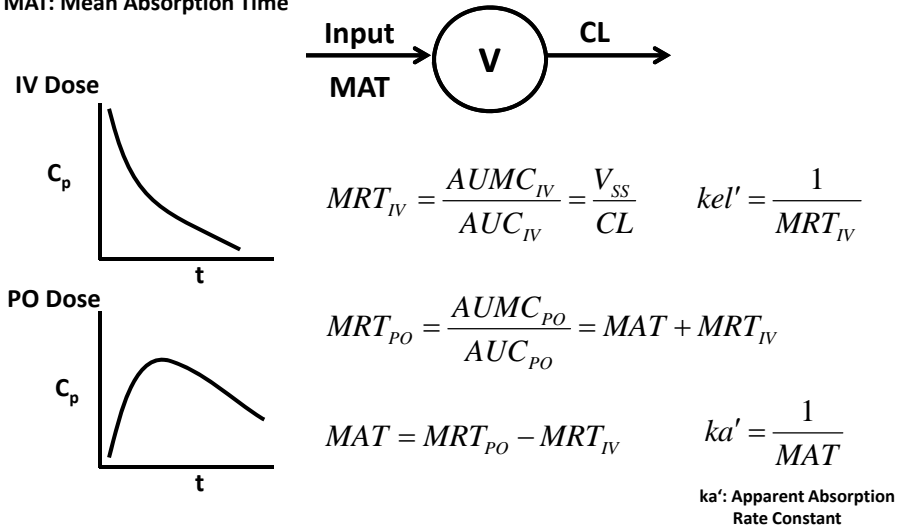
$$V_{ss} = MRT \cdot CL$$

- Physiological Models

$$V_{ss} = V_{\text{plasma}} + \sum P_i \cdot V_{\text{tissue}}$$

Mean Residence Time: Drug Absorption

MAT: Mean Absorption Time



Limitations of Noncompartmental Analyses

- While AUC and AUMC are easily generated, they are **UNABLE** to visualize or predict plasma concentration-time profile for other dosing regimens.
- Requires the kinetics to be linear and stationary (i.e., time-independent) for simple applications.

Summary: Noncompartment Methods

- Calculation of AUC, AUMC, and MRT are valuable initial steps in PK data analysis.
- Calculation of
 $CL = \text{Dose}/AUC$
is relevant for all traditional PK models regardless of numbers of exponentials.
- Calculation of
 $V_{ss} = MRT \cdot CL$
is easy and relevant for all linear models.